

CISM International Centre for Mechanical Sciences 546
Courses and Lectures

Markus J. Buehler
Roberto Ballarini
Editors

Materiomics: Multiscale Mechanics of Biological Materials and Structures



International Centre
for Mechanical Sciences



Springer

CISM Courses and Lectures

Series Editors:

The Rectors

Friedrich Pfeiffer - Munich
Franz G. Rammerstorfer - Wien
Elisabeth Guazzelli - Marseille

The Secretary General
Bernhard Schrefler - Padua

Executive Editor
Paolo Serafini - Udine



The series presents lecture notes, monographs, edited works and proceedings in the field of Mechanics, Engineering, Computer Science and Applied Mathematics.

Purpose of the series is to make known in the international scientific and technical community results obtained in some of the activities organized by CISM, the International Centre for Mechanical Sciences.

International Centre for Mechanical Sciences

Courses and Lectures Vol. 546

For further volumes:
www.springer.com/series/76

Markus J. Buehler and Roberto Ballarini
Editors

**Materiomics:
Multiscale Mechanics of
Biological Materials and
Structures**



Springer

Editors

Markus J. Buehler

Civil and Environmental Department, Massachusetts Institute of Technology,
Cambridge, MA, USA

Roberto Ballarini

Department of Civil Engineering, University of Minnesota, Minneapolis, USA

ISSN 0254-1971

ISBN 978-3-7091-1573-2 ISBN 978-3-7091-1574-9 (eBook)

DOI 10.1007/978-3-7091-1574-9

Springer Wien Heidelberg New York Dordrecht London

© CISM, Udine 2013

This work is subject to copyright. All rights are reserved by the Publisher, whether the whole or part of the material is concerned, specifically the rights of translation, reprinting, reuse of illustrations, recitation, broadcasting, reproduction on microfilms or in any other physical way, and transmission or information storage and retrieval, electronic adaptation, computer software, or by similar or dissimilar methodology now known or hereafter developed. Exempted from this legal reservation are brief excerpts in connection with reviews or scholarly analysis or material supplied specifically for the purpose of being entered and executed on a computer system, for exclusive use by the purchaser of the work. Duplication of this publication or parts thereof is permitted only under the provisions of the Copyright Law of the Publisher's location, in its current version, and permission for use must always be obtained from Springer. Permissions for use may be obtained through RightsLink at the Copyright Clearance Center. Violations are liable to prosecution under the respective Copyright Law.

The use of general descriptive names, registered names, trademarks, service marks, etc. in this publication does not imply, even in the absence of a specific statement, that such names are exempt from the relevant protective laws and regulations and therefore free for general use.

While the advice and information in this book are believed to be true and accurate at the date of publication, neither the authors nor the editors nor the publisher can accept any legal responsibility for any errors or omissions that may be made. The publisher makes no warranty, express or implied, with respect to the material contained herein.

All contributions have been typeset by the authors

Printed in Italy

Printed on acid-free paper

Springer is part of Springer Science+Business Media (www.springer.com)

PREFACE

This book contains lecture notes from leading researchers in the field of mechanical sciences of biological materials and structures, with a focus on the behavior of biological materials under extreme physical, chemical, physiological and disease conditions, as well as on biomimetic and bioinspired material development for technological applications. To provide a thorough foundation for this research, the course will focus on the integration of advanced experimental, computational and theoretical methods applied to the study of biological materials across disparate length- and time-scales. Specific attention is paid to the integration of theoretical, computational and experimental tools that could be used to assess structure-process-property relations and to monitor and predict mechanisms associated with the function and failure of biological materials and structures composed of them.

The chapters provide overviews of emerging fields of research and highlight important challenges and opportunities. Hence, the three core objectives of this book are to: (1) Provide a clear description of methods and tools, (2) Present case studies that demonstrate the impact of multiscale modeling approaches, and to (3) Provide a carefully selected list of core references and citations for the interested reader. The case studies include the analysis of key biological materials, the biodegradation of implanted synthetics, the transfer of biological material principles towards bioinspired applications, and the exploration of diseases in which material failure plays a critical role. The approaches presented in this book emphasize the fundamental principles of physics, chemistry and mechanics, and they rely on quantum mechanics, molecular dynamics and continuum analyses. The use of basic sciences creates a powerful common platform regardless of the specific material system considered, and can therefore be transferred to other types of materials and structures.

The editors of this volume would like to thank the CISM team for their help and support in preparing this book. They are also grateful to the contributors of the various chapters for their time and efforts, and acknowledge the support of their research on the mechanical behavior of materials and structures over the years from the National Science Foundation, the Army Research Office, the Office of Naval

*Research, DARPA, the Air Force Office for Scientific Research, and
the National Institutes of Health.*

Roberto Ballarini and Markus Buehler

CONTENTS

| | |
|--|-----|
| Introduction <i>by R. Ballarini and M.J. Buehler</i> | 1 |
| Multiscale Modeling of Biomaterials and Tissues <i>by A. Gautieri and M.J. Buehler</i> | 13 |
| Microelectromechanical Systems (MEMS) Platforms for Testing the Mechanical Properties of Collagen Fibrils <i>by R. Ballarini and H. Kahn</i> | 57 |
| Multiscale Modeling of Diffusion Phenomena in Polymers <i>by A. Redaelli, S. Vesentini, A. Gautieri and P. Zunino</i> .. | 71 |
| Advances in Experimental Cell Biology and Cell-Material Interactions <i>by C.M. Copley, S. Wegner, M. Streichfuss and J.P. Spatz</i> | 87 |
| Microfluidic Platforms for Human Disease Cell Mechanics Studies <i>by E.W. Majid and C.T. Lim</i> | 107 |
| Continuum Analyses of Structures Containing Cracks <i>by R. Ballarini</i> | 121 |

Introduction

Roberto Ballarini ^{*} and Markus Buehler [†]

^{*} Department of Civil Engineering, University of Minnesota, Minneapolis, USA

[†] Department of Civil and Environmental Engineering, Massachusetts Institute of Technology, Cambridge, USA

1 The promise of multiscale modeling and bioinspired engineering

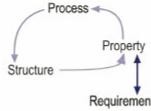
The field of multiscale mechanics has witnessed an exciting development over the past decades, culminating in recent years in breakthrough discoveries that have blurred the boundaries between living and synthetic materials, and have enabled the first wave of high-impact applications of new materials and structures in biomedical, energy and structural engineering applications. Multiscale modeling offers promise for facilitating the creation of engineered materials and structures with properties that resemble those of biological systems, in particular the ability to self-assemble, to self-repair, to adapt and evolve, and to provide multiple functions that can be controlled through external cues. In addition to their potential for enabling the realization of advanced technological applications, the challenges posed by the complex behavior of hierarchical tissues and cells in biological systems represent terrific opportunities to open new chapters in the development of the mechanical sciences. It is remarkable how the mechanics practiced by da Vinci, Galileo, Newton and other great scientists has evolved to a point where now it interconnects intimately with the life sciences, and that it could ultimately contribute to the solutions of critical problems encountered in such disparate fields as medicine and the aging infrastructure.

Yet, in spite of significant advancements in the study of biological materials in the past decade, a lack of sufficient understanding of the fundamental physics of many phenomena in biology is hindering our progress towards the building of sufficiently robust models, simulation tools and experimentation. For example, the understanding of the mechanisms of failure in biological systems remains elusive, including those involved in the breakdown of diseased tissue, the failure of biological components due to injuries, and the ability of biological systems to mitigate adverse effects of damage through

self-healing mechanisms. The cost-effective manufacturing of bioinspired products is also an enormous challenge, because humans have traditionally relied on top-down fabrication paradigms that simply cannot be used to efficiently produce the highly hierarchical structures that *Nature* builds from the bottom-up. Improved understanding of how biology originates from the molecular scale and proceeds to genes (DNA), proteins, tissues, organs and organisms can guide our development of self-assembly technologies that will allow mass production and utilization of bioinspired materials for daily life applications like consumer products, medical devices and large-scale systems in the aerospace, defense and building industries.

The highly complex nature of biological structures, which involve multiphysics and multiple length and time scales, has inspired the new field of study referred to as materiomics, which is defined in the next section and is reflected by the contents of this book.

Material science paradigm linking structure, process and property:



Paradigm adapted to biological material, encompassing a more complex materiomie:

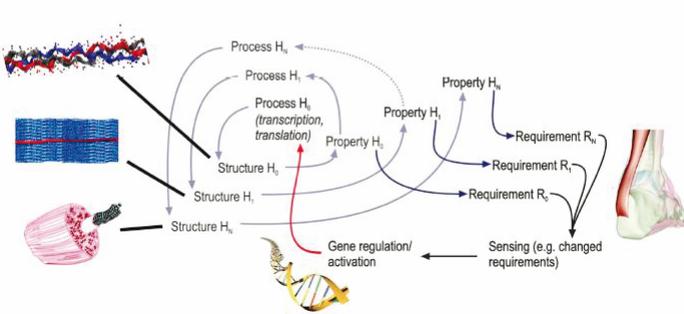


Figure 1. Schematic representing the materiomics approach (Cranford and Buehler (2012)).

2 Materiomics

What is materiomics? As illustrated schematically in Figure 1, it is an approach rooted in physics that extends the structure-process-property-

requirement paradigm that has been developed by materials scientists to the analysis of highly complex biological and synthetic materials and structures. The schematic emphasizes that materiomics is a holistic systems approach to the theoretical, computational and experimental study of materials that aims to identify links between processes, structures, and properties across multiple scales, from nano to macro. The integrated view and description of the building blocks of a hierarchical structure and their fundamental interactions is referred to as the material's materioeme. Materiomics thus provides a systematic description of universal mechanisms by which complex system functionality and failure can be explained from the materioeme. As sketched in Figure 2, similar to the way music is created from a finite number of musical notes, the relationships between form and function found in natural materials provide the mechanistic basis to explain the remarkable mechanical properties of materials like nacre, bone, spider silk and collagen. For example, it has been determined that the toughness of bone and of sea shells of the crossed-lamellar type are the result of multiple and synergetic toughening mechanisms made possible by a half-dozen distinct microstructural features (Kamat et al. (2000); Ballarini et al. (2005)). In fact, for bone, sea shells and most other biological objects the traditional concepts of "structure" and "material" are blurred, and integrated in a vision that derives functional properties by systematically and strategically adapting multiple levels across numerous length- and time-scales (Figure 2). This viewpoint extends our current ability to engineer structures to the desired scale, and requires a multidisciplinary treatment of problems to incorporate physics, chemistry and advanced mathematics to develop complex models to design and predict performance.

New approaches that take advantage of mathematical tools such as material ologs (Spivak et al. (2011)) are important in arriving at a systematic analysis that reduces complexity to distill the essential features. Moreover, a range of experimental and computational tools is needed to measure and produce structures and properties at these variegated length- and time scales. A summary of key computational methods, synthesis, processing and experimental techniques is provided in Figure 3. It is evident that with modern tools a very broad range of scales can be seamlessly explored, thus allowing the realization of realistic multiscale analysis. Figure 4 depicts an impressive example of a precise experimental analysis of collagen microfibrils using the microtechnology-based material testing described in Chapter 3, something that would have been impossible just a few years ago.

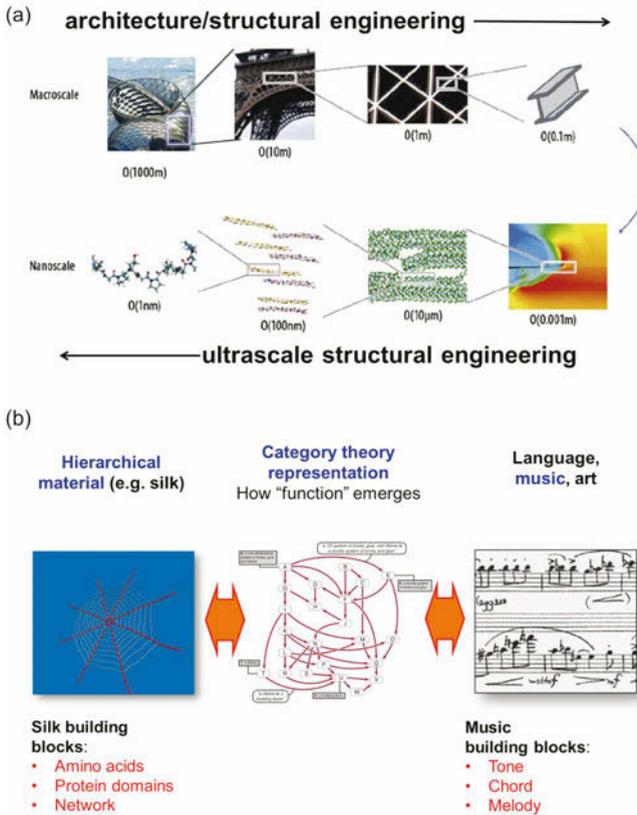


Figure 2. Common principles of biological and bioinspired material design, showing the merger of “structure” and “material” across different length scales in hierarchical materials (Buehler and Ackbarow (2007)).

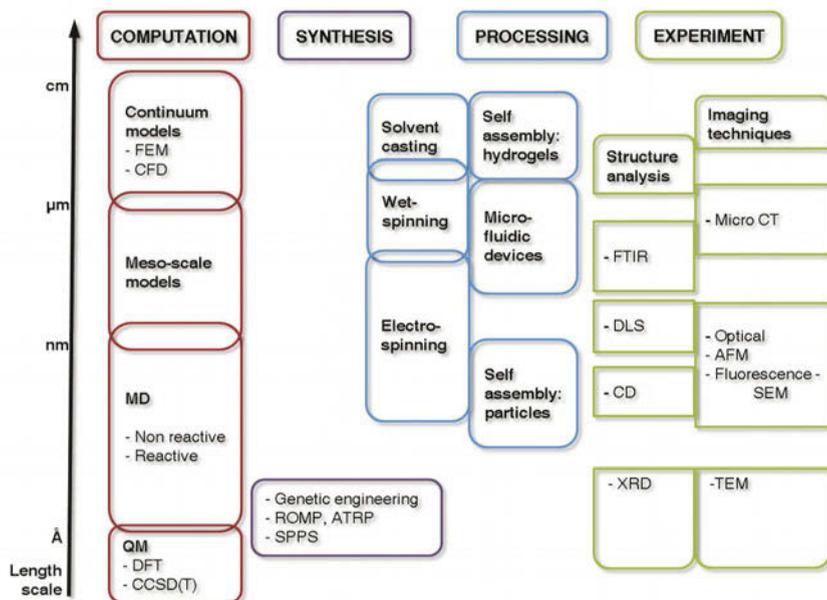


Figure 3. Overview of various computational and experimental tools, including synthesis, processing and imaging/manipulation techniques. The emergence of tools operating at different length scales now enables the analysis of materials across all relevant scales (Gronau et al. (2012)).

3 Motivation for studying biological structures: The superior performance of natural structures conferred by their hierarchical designs

Why should humans study biological structures and paradigms? Because *Nature* has created an extremely large number of high-performance prototypes that humans can reverse engineer and in turn use as inspirations for creating synthetic products with similar superior performances. This section focuses on but one strategy used by *Nature* to create materials and structures whose survival requires superior mechanical properties and structural behavior, namely highly hierarchical design.

The structures created by organisms, although made from rather mundane materials, show impressive properties that are clearly well-suited for

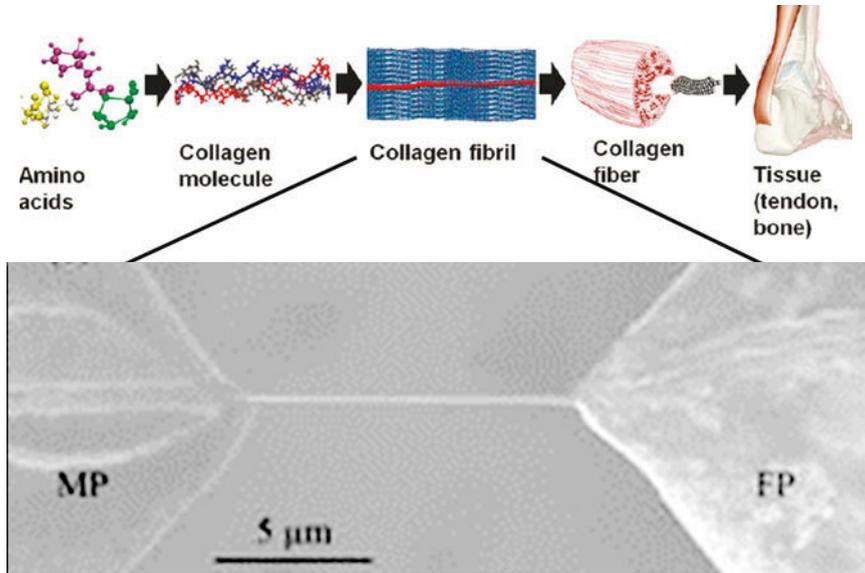


Figure 4. Example of advanced experimentation applied to test the nanomechanics of individual collagen fibrils. Results from such experiments can be compared to molecular modeling and enable us to ask fundamental questions about the physiology and disease of key construction materials in nature (adapted from Eppell et al. (2006)).

their intended functions. Structure/function/performance correlations have been assumed by scientists to be a result of evolutionary pressures inherent in natural selection. While proponents of “intelligent design” offer other explanations, the diversity of microstructure in structures such as molluscan shells and bone and their remarkable mechanical properties and self-healing mechanisms testifies to the flexibility and power of this approach. *Nature* achieves robust structures using as little mass as possible, through judicious arrangements of mundane polymeric and ceramic components. Be they primarily ceramic (tooth enamel, mollusc shell), polymeric (insect exoskeleton, plant cell walls), or more evenly balanced composites (antler, bone), biological materials are virtually all composites utilizing different proportions of the basic components and a variety of hierarchical structural architectures.

It is very instructive to compare the mechanical properties of biological structures with materials created by humans through the performance index paradigm pioneered by Ashby (Ashby (1992)). First, a brief primer on basic structural mechanics. Consider the simple extension of a rod of length, L , and cross-sectional area, A , made of a material with density, ρ (Figure 5). In terms of the applied force, F , and the elongation, δ , the stress and strain are defined as $\sigma = \frac{F}{A}$ and $\varepsilon = \frac{\delta}{L}$. For most engineering materials, the relation between σ and ε is linear at small values of strain, with a slope defined as the elastic (Young's) modulus, E . At the elastic limit, σ_f , the curve ends abruptly for brittle materials and is nonlinear for ductile materials up to the ultimate stress required to fracture the rod, σ_u . The area under the linear part of the curve up to a given strain, $\frac{\sigma_f^2}{2E}$, is defined as the elastic strain energy density and represents the potential energy conferred to the rod by the work performed by the applied force. If the strain is limited to values less than the yield strain, $\varepsilon_f = \frac{\sigma_f}{E}$, then the tie will return to its original length upon removal of the force. This behaviour is referred to as elastic, in that no energy is dissipated during a loading-unloading cycle. The total area under the $\sigma - \varepsilon$ curve represents the work done by the force to fracture the rod into two pieces; the work of fracture is defined as this work divided by the area of the surfaces created by fracturing the rod into two pieces.

If a relatively brittle structure contains a crack-like flaw and is treated as linear elastic, the stresses along the crack front are singular and therefore cannot be directly used to predict load carrying capacity. Instead, the force required to fracture the structure is determined by the stress intensity factor, K , which characterizes the stress and strain intensities in the vicinity of the crack front. The stress intensity factor depends on the geometry of the structure, the type of loading, and the specific crack shape; according to linear elastic fracture mechanics theory the crack will extend across the specimen when K reaches a critical value defined as the fracture toughness, K_c . The stress intensity factor is directly related to J , the energy available to overcome the material's resistance to crack extension, by the equation $K = \sqrt{EJ}$. Therefore the fracture toughness can be expressed in terms of the energy required to create the fracture surfaces, J_c , by the relation $J_c = \frac{K_c^2}{E}$.

Quantitative comparisons between materials can be made using the concept of material performance indices, parameters that quantify a material's ability to perform a certain function. The higher the value of the index, the better suited is the material for a given application. For a thorough discussion of the mechanical properties of natural materials and the origins of their superiority, the reader is referred to Ashby et al. (1995) and Wegst and Ashby (2004). Here we borrow from their discussions.

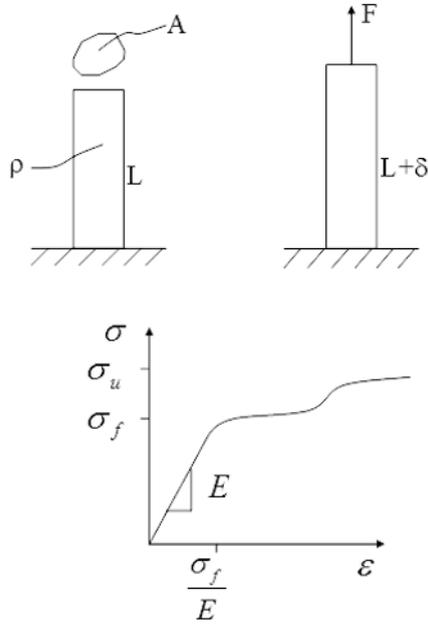


Figure 5. Simple elongation experiment and representative stress-strain curve.

Table 1. Performance indices for different types of structural elements.

| Design | Tie in tension | Beam in flexure | Plate in flexure |
|--|--|--|--|
| Maximum strength to weight | $\frac{\sigma_f}{\rho}$ | $\frac{\sigma_f^{2/3}}{E^{1/3}}$ | $\frac{\sigma_f^{1/2}}{E^{1/3}}$ |
| Maximum stiffness to weight | $\frac{E}{\rho}$ | $\frac{E^{1/2}}{E^{1/2}}$ | $\frac{E^{1/3}}{E^{1/3}}$ |
| Large recoverable deformation | $\frac{\sigma_f}{E_f}$ | $\frac{\sigma_f}{E_f}$ | $\frac{\sigma_f}{E_f}$ |
| Spring with minimum volume | $\frac{\sigma_f^2}{E}$ | $\frac{\sigma_f^2}{E}$ | $\frac{\sigma_f^2}{E}$ |
| Fracture safe displacement controlled design | $\left(\frac{J_c}{E}\right)^{\frac{1}{2}}$ | $\left(\frac{J_c}{E}\right)^{\frac{1}{2}}$ | $\left(\frac{J_c}{E}\right)^{\frac{1}{2}}$ |

Consider first the minimum weight design of three simply loaded structures; a rod in tension, a flexed beam, and a flexed plate. The first two rows of Table 1 list the performance indices relevant to a minimum weight design of these structures that does not specify the shape of the element's cross-section. The fact that the most efficient material for a strong and light tie (or similarly stiff and light) subjected to simple elongation is the one that possesses the largest value of $\frac{\sigma_f}{\rho}$ (or similarly $\frac{E}{\rho}$) is perhaps obvious and can be guessed by someone that has never taken a course in mechanics. However, those that have studied structural mechanics know that beam and plates experience spatially varying stress and strain distributions that lead to performance indices that involve different rational exponents to the strength and stiffness.

Table 2. Stiffness to weight performance indices. The parentheses reflect the elastic modulus along the stiffer direction, and therefore are not representative of a stiff plate in bending that requires equal moduli in all directions (adapted from Ashby et al. (1995); Wegst and Ashby (2004)).

| Material | E/ρ (GPa/Mg/m ³) | $E^{\frac{1}{2}}/\rho$ (GPa ^{$\frac{1}{2}$} /Mg/m ³) | $E^{\frac{1}{3}}/\rho$ (GPa ^{$\frac{1}{3}$} /Mg/m ³) |
|-----------------|-----------------------------------|--|--|
| Palm (Iriartea) | 23 | 12.5 | (10.1) |
| Mild steel | 27 | 1.8 | (0.8) |
| Balsa wood | 20 | 14.1 | (12.6) |

Consider specific materials. Table 2 shows that for the stiff and light design, the performance index of mild steel is comparable (actually slightly higher) to that of the two representative woods. However, steel is not nearly as efficient as Palm or Balsa for beams or plate elements subjected to flexure. This data suggests that the various hierarchical microstructures of wood have evolved to ensure that trees are efficient in their response to the principal loads they must carry; bending of branches under their own weight and bending of trunks under wind loads. Similar insights are provided by Table 3 for the strong and light design criterion.

We now turn our attention to material choices for an elastic hinge, a component that is required to undergo relatively large deformation when loaded, and to return to its original shape when the load is removed. The performance index for the design of elastic hinges is $\frac{\sigma_f}{E}$, and it as listed in Table 4, leather, cartilage, and to a lesser extent, skin, are the best choices. To man's credit, rubber edges out its biological counterparts, although rubber is not usually thought of as a bioinspired material.

Table 4 also shows that silk fibre is the top choice for springs that are required to absorb the most energy per unit volume. In fact, it out performs

Table 3. Strength to weight performance indices. The parentheses reflect the elastic modulus along the stiffer direction, and therefore are not representative of a stiff plate in bending that requires equal moduli in all directions (adapted from Ashby et al. (1995); Wegst and Ashby (2004)).

| Material | σ_f/ρ (GPa/Mg/m ³) | $\sigma_f^{2/3}/\rho$ (GPa ^{2/3} /Mg/m ³) | $\sigma_f^{1/2}$ (GPa ^{1/2} /Mg/m ³) |
|------------|--|--|---|
| Mild steel | 51 | 6.9 | 2.5 |
| Balsa wood | 160 | 64 | (40.0) |

man-made spring steel, and the natural elastic hinges leather and cartilage by significant margins. Its molecular design guarantees that silk can absorb, without fracturing, the energy introduced by the excursions of the spider and/or the desperate movements of its entangled prey.

Table 4. Performance indices relevant to hinges and springs (adapted from Ashby et al. (1995); Wegst and Ashby (2004)).

| Material | σ_f/E | σ_f^2/E (MJ/m ³) |
|-------------------|--------------|-------------------------------------|
| Spring steel | 0.01 | 19.0 |
| Soft butyl rubber | 1.40 | 19.6 |
| Single silk fiber | 0.14 | 290.0 |
| Cartilage | 1.00 | 10.0 |
| Skin | 0.25 | 2.5 |
| Leather | 1.00 | 45.0 |

The last example involves cracked structures. Consider the specific case of choosing a material for a cracked structure that is required to survive large elastic deformation. Table 5 indicates that skin has the best performance index, despite having a much lower fracture toughness than steel or highly mineralized mollusc shell. Interestingly, the microstructural design of skin may have evolved to make it ideally suited for being stretched around our knuckles and elbows without tearing. We could not enjoy such movements if our skin had the fracture properties of man-made alloys or other biological materials.

The biological materials just described can therefore be considered prototypes of successful structural designs that *Nature* has provided to gratis and that can inspire us to create our own tailor made materials with similar performances. The major challenge is the development of methods for fabricating such highly hierarchical structures.

Nature is indeed impressive and inspiring.

Table 5. Performance indices for structures containing cracks (adapted from Ashby et al. (1995); Wegst and Ashby (2004)).

| Material | $K_c = (EJ_c)^{\frac{1}{2}} \text{ (MPa} - m^{\frac{1}{2}})$ | $\left(\frac{J_c}{E}\right)^{\frac{1}{2}} \text{ (mm}^{\frac{1}{2}})$ |
|---------------|--|---|
| Mollusc shell | 9.5 | 0.4 |
| Mild steel | 90.0 | 0.4 |
| Skin | 0.4 | 38.7 |

Bibliography

- M.F. Ashby. *Materials selection in mechanical design*. Pergamon Press, 1992.
- M.F. Ashby, L.J. Gibson, U. Wegst, and R. Olive. The mechanical properties of natural materials. i. material property charts. *Proc. R. Soc. Lond. A*, 450:123–140, 1995.
- R. Ballarini, R. Kayacan, F.J. Ulm, T. Belytschko, and A.H. Heuer. Biological structures mitigate catastrophic failure through various strategies. *International Journal of Fracture*, 135:187–197, 2005.
- M.J. Buehler and T. Ackbarow. Fracture mechanics of protein materials. *Materials Today*, 10(9):46–58, 2007.
- S. Cranford and M.J. Buehler. *Biomateriomics*. Springer, 2012.
- S. Eppell, B. Smith, H. Kahn, and R. Ballarini. Anano measurements with micro devices: Mechanical properties of hydrated collagen fibrils. *Journal of the Royal Society Interface*, 3:117–121, 2006.
- G. Gronau, S. Tarakkad Krishnaji, M.E. Kinahan, T. Giesa, J.Y. Wong, D.L. Kaplan, and M.J. Buehler. A review of biopolymer structure-process-property relationships at multiple scales via integration of modeling and experimentation. *Biomaterials*, accepted for publication, 2012.
- S. Kamat, X. Su, R. Ballarini, and A.H. Heuer. Structural basis for the fracture toughness of the shell of the conch strombus gigas. *Nature*, 405: 1036–1040, 2000.
- D. Spivak, T. Giesa, E. Wood, and M.J. Buehler. Fracture mechanics of protein materials. *PLoS ONE*, 6(9):e23911, 2011.
- U.G.K. Wegst and M.F. Ashby. The mechanical efficiency of natural materials. *Philosophical Magazine*, 21:2167–2181, 2004.

Multi-scale modeling of biomaterials and tissues

Alfonso Gautieri^{1, 2} Markus J. Buehler^{1, *}

¹ Civil and Environmental Department, Massachusetts Institute of Technology,
Cambridge, MA, USA

² Department of Bioengineering, Politecnico di Milano, Italy

Abstract

Computer simulation has emerged as a powerful tool to investigate and design materials without ever making them. Predicting the properties and behavior of materials by computer simulation from the bottom-up perspective has long been a vision of computational materials scientists and, as computational power increases, modeling and simulation tools are becoming crucial to the investigation of material systems. The key to achieving this goal is using hierarchies of paradigms that seamlessly connect quantum mechanics to macroscopic systems. Particular progress has been made in relating molecular-scale chemistry to mesoscopic and macroscopic material properties essential to define the *materiome*. This chapter reviews large-scale atomistic and coarse-grain modeling methods commonly implemented to investigate the properties and behavior of natural and biological materials with nanostructured hierarchies. We present basic concepts of hierarchical multiscale modeling capable of providing a bottom-up description of chemically complex materials and some example applications related to the study of collagen material at different hierarchical levels.

1 Introduction to the multi-scale modeling paradigm

In recent years, researchers consider computer simulations as a tool to design new materials, new structures, or to develop new drugs, without the need to synthesize them. A vision of materials scientists has long been to

* Corresponding author at: Laboratory for Atomistic and Molecular Mechanics, Department of Civil and Environmental Engineering, Massachusetts Institute of Technology, 77 Massachusetts Ave., Room 1-235A&B, Cambridge, MA, USA. Tel.: +1-617-452-2750. E-mail address: mbuehler@MIT.EDU (M.J. Buehler).